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Hirahara

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(54) **PCR METHOD AND PCR DEVICE**
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C12P 19/34 (2006.01)
B01L 7/00 (2006.01)
B01L 3/00 (2006.01)
C07H 21/02 (2006.01)
C07H 21/04 (2006.01)
(52) **U.S. Cl.**
CPC **B01L 7/52** (2013.01); **B01L 2300/0645** (2013.01); **B01L 2300/0832** (2013.01); **B01L 3/5027** (2013.01); **B01L 2300/0816** (2013.01); **B01L 2300/1833** (2013.01); **B01L 2400/0472** (2013.01); **B01L 2400/0487** (2013.01); **C12Q 1/686** (2013.01)
(58) **Field of Classification Search**
CPC C12Q 1/686; C12Q 2565/607; B01L 2300/0816; B01L 2300/1833; B01L 2400/0472; B01L 2400/0487; B01L 3/5027; B01L 7/52
See application file for complete search history.

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(57) **ABSTRACT**

Provided on an inner surface of a container to carry out polymerase chain reaction (PCR) are an electrode pair **22** to be disposed to face each other with a gap along a flow of a reaction solution interposed therebetween, and an AC voltage is applied to the electrode pair **22** to make an AC current flow through the reaction solution, whereby Joule heat is generated to control the reaction solution in temperature. Accordingly, a PCR method and a PCR device that allow generating sufficient Joule heat for a PCR cycle even when an applied voltage is low, and do not electrolyze a reaction solution even by making an electric current flow through the reaction solution can be provided.

15 Claims, 6 Drawing Sheets

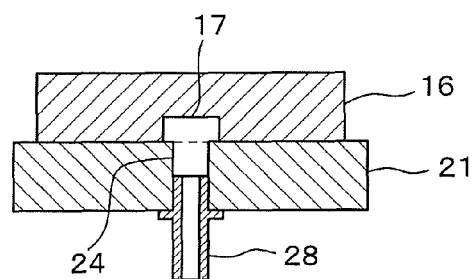


FIG. 2

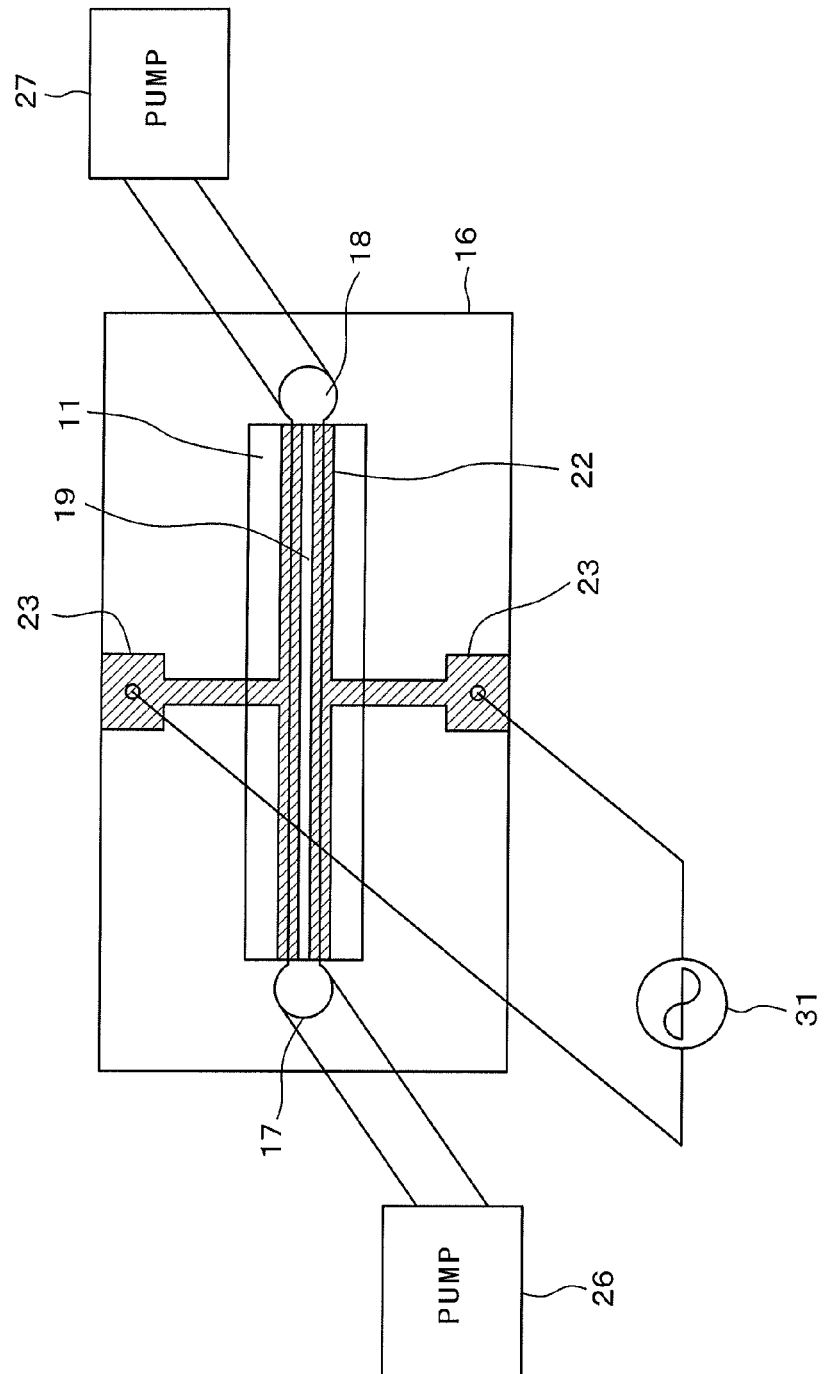


FIG. 3

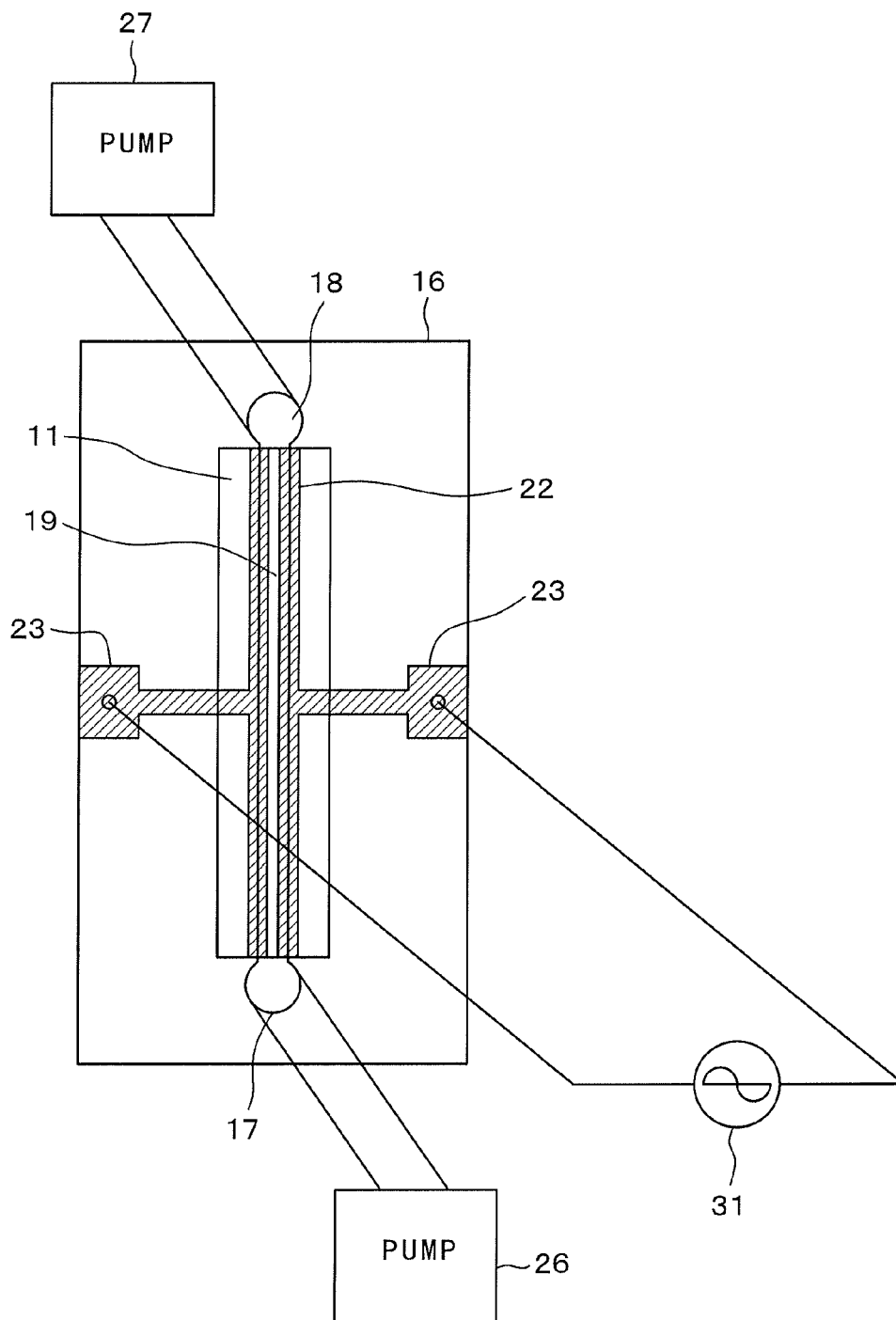


FIG. 4

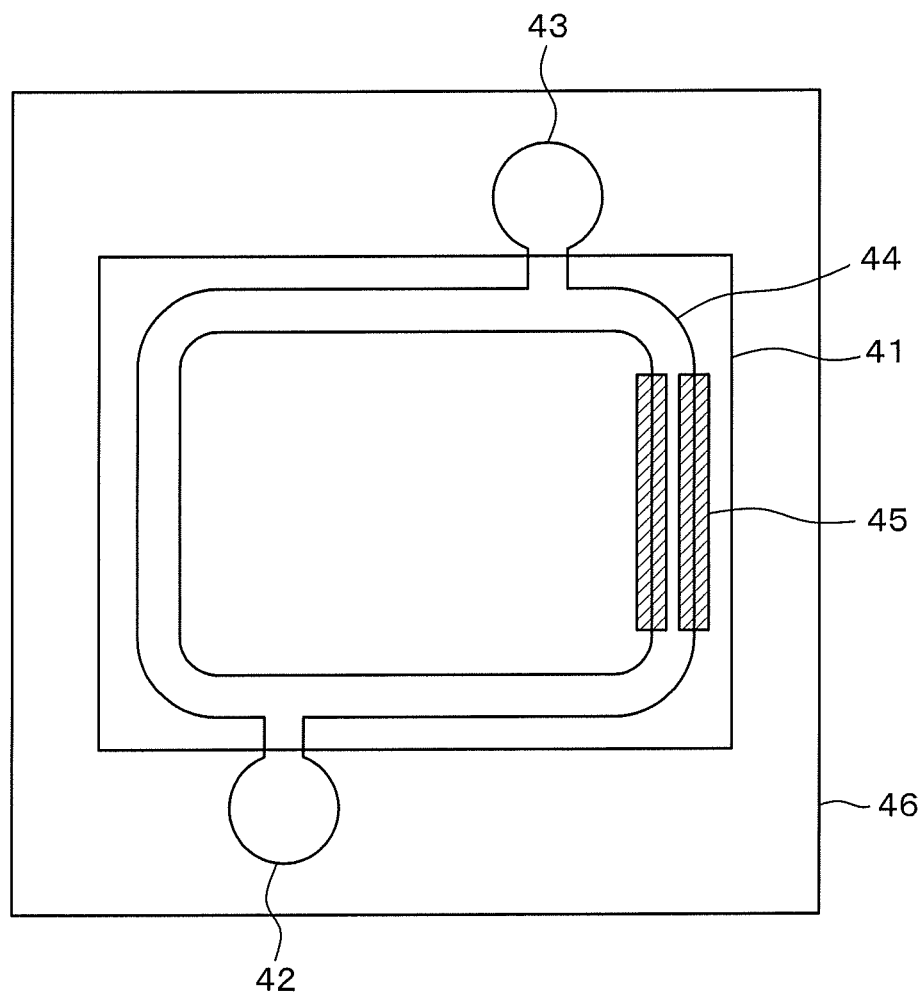


FIG. 5

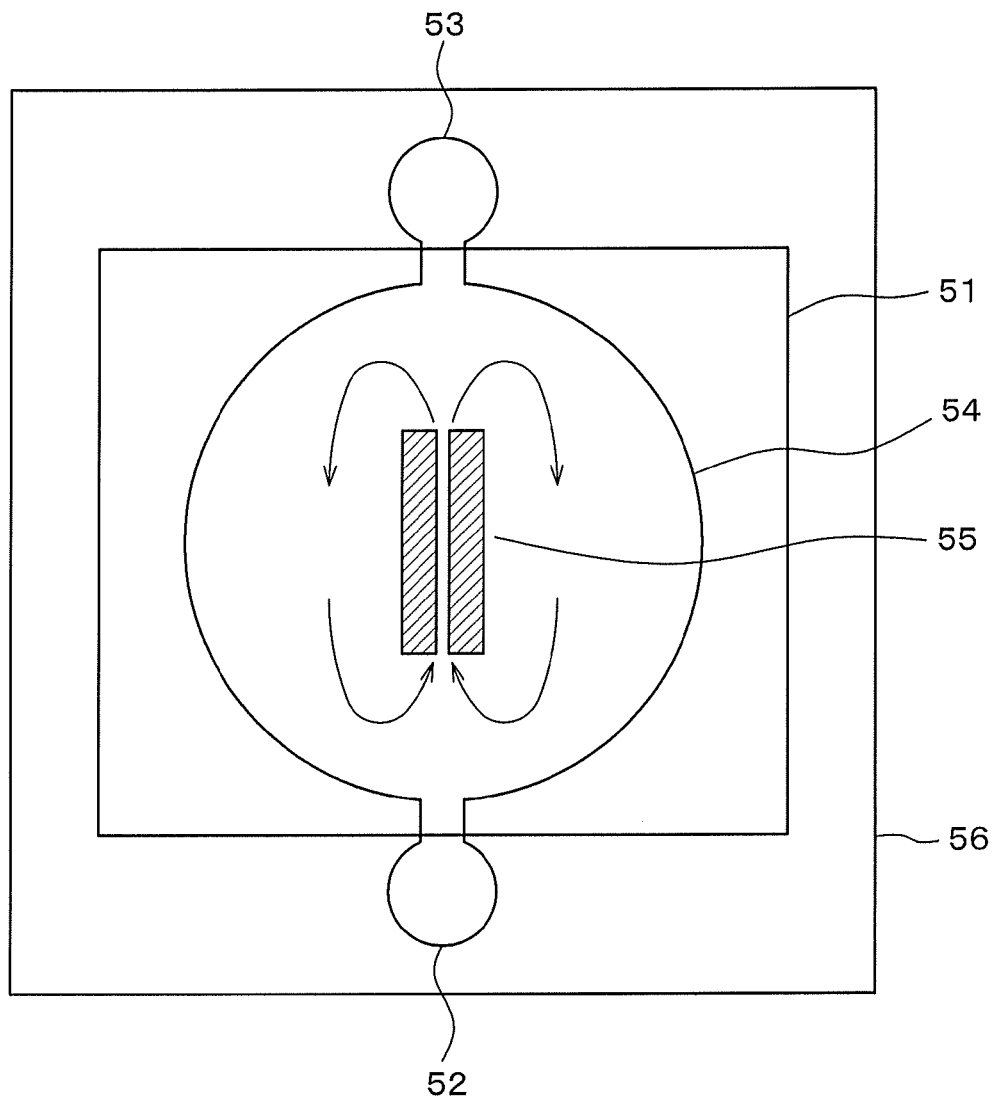


FIG. 6A

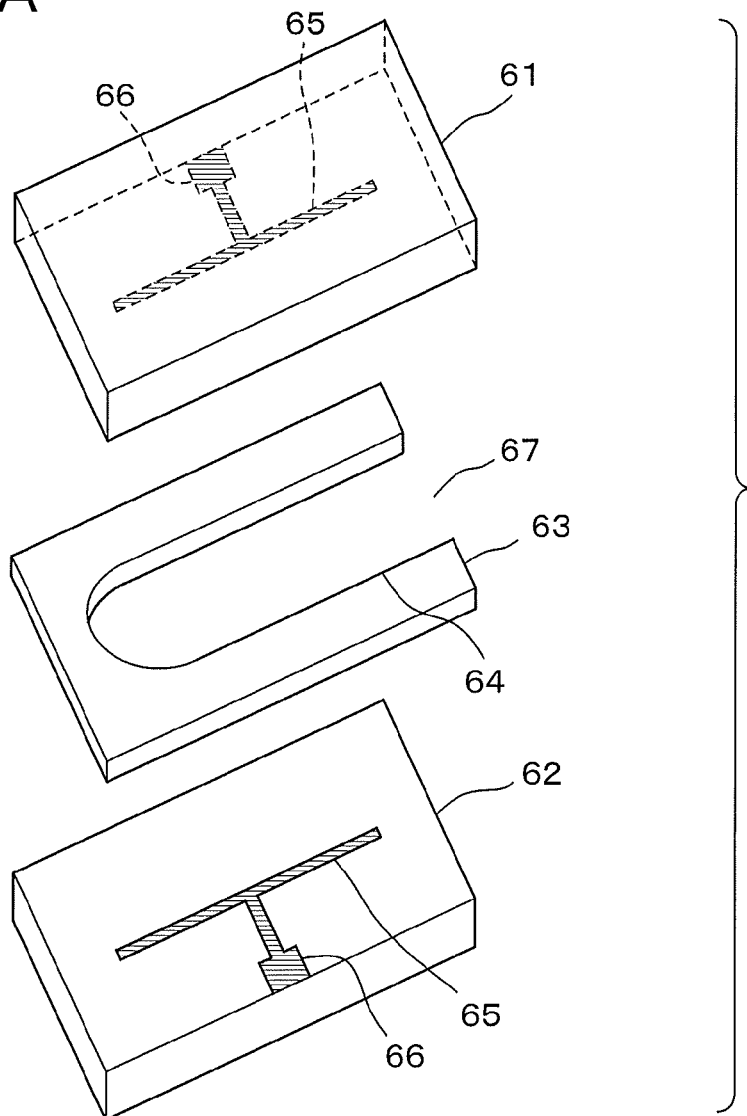
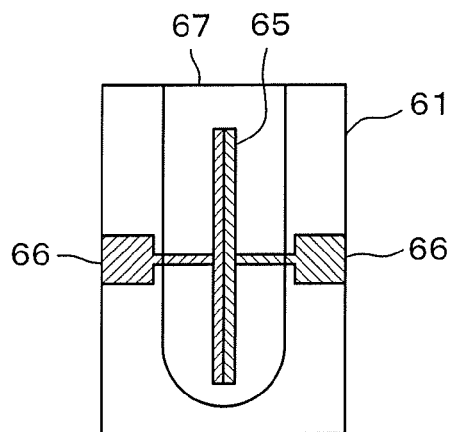


FIG. 6B



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PCR METHOD AND PCR DEVICE

TECHNICAL FIELD

The present invention relates to a PCR (polymerase chain reaction) method and a PCR device, and particularly, to a PCR method and a PCR device that have a high response rate to temperature control.

BACKGROUND ART

A conventional PCR method uses an external heater as a means for raising the temperature of a reaction solution for a PCR cycle, and heat of the heater is transmitted to the reaction solution via a wall of a reaction container to heat the reaction solution. However, in this case, the wall is first heated, and the reaction solution is heated by heat of the wall, and thus the response rate of temperature control is low, and heat is diffused along the wall to result in poor energy efficiency.

Therefore, it has been proposed to make electric current flow through a reaction solution to directly heat the reaction solution by Joule heat (refer to, for example, Non Patent Literature 1).

CITATION LIST

Non Patent Literature

[Non Patent Literature 1] Guoqing Hu et al., "Electrokinetically controlled real-time polymerase chain reaction in microchannel using Joule heating effect", *Analytica Chimica Acta*, vol. 557, (2006) pp. 146-151.

SUMMARY OF INVENTION

Technical Problem

However, because the conventional PCR method using Joule heating makes a DC current flow through a reaction solution, the reaction solution is electrolyzed to produce unnecessary gas on the periphery of the electrodes, and produce unnecessary acidic and alkaline solutions, and thus addressing the same is necessary, and because a voltage is applied to both ends of a long channel, a high voltage must be applied to generate necessary Joule heat, causing a large load on the circuit.

In view of the above problems, it is an object of the present invention to provide a PCR method and a PCR device that allow generating sufficient Joule heat for a PCR cycle even when an applied voltage is low, and do not electrolyze a reaction solution even by making an electric current flow through the reaction solution.

Solution to Problem

A PCR method of the present invention is a method of providing, on an inner surface of a container to carry out polymerase chain reaction (PCR), an electrode pair to be disposed to face each other with a gap along a flow of a reaction solution interposed therebetween, and applying an AC voltage to the electrode pair to make an AC current flow through the reaction solution, thereby generating Joule heat to control the reaction solution in temperature.

Moreover, a PCR device of the present invention comprises: a container to carry out polymerase chain reaction (PCR); an electrode pair disposed to face each other with a gap along a flow of a reaction solution interposed therebe-

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tween; and a control unit which applies an AC voltage to the electrode pair to make an AC current flow through the reaction solution, thereby generating Joule heat to control the reaction solution in temperature.

Moreover, as a result of the container being a tubular channel, as compared with a slight amount of reaction solution within the channel, large electrodes can be used, and thus the response rate of the reaction solution temperature to voltage application can be increased.

Moreover, as a result of the channel being vertically oriented, an upward flow of the reaction solution by Joule heating can be used.

Moreover, as a result of the container being a flat chamber which is vertically erected, and the electrode pair being disposed to face each other with a vertical gap interposed therebetween on an inner surface of one of the sidewalls of the chamber, the reaction solution can be circulated within the chamber to perform a PCR cycle.

Moreover, as a result of the container being a flat chamber which is vertically erected, and the electrode pair being disposed to face each other, with the chamber interposed as a gap therebetween, on an inner surface of one of the sidewalls of the chamber and an inner surface of the other sidewall, the reaction solution can also be circulated within the chamber to perform a PCR cycle.

Advantageous Effects of Invention

The present invention allows generating sufficient Joule heat for a PCR cycle even when an applied voltage is low, and does not electrolyze a reaction solution even by making an electric current flow through the reaction solution.

BRIEF DESCRIPTION OF DRAWINGS

FIG. 1A is an exploded perspective view depicting a configuration of a reaction container of a PCR device according to Example 1 of the present invention.

FIG. 1B is a sectional view of FIG. 1A.

FIG. 2 is a top view of the reaction container of the PCR device according to Example 1 of the present invention and a view depicting a peripheral configuration thereof.

FIG. 3 is a top view of a reaction container of a PCR device according to Example 2 of the present invention and a view depicting a peripheral configuration thereof.

FIG. 4 is a front view of a reaction container of a PCR device according to Example 3 of the present invention.

FIG. 5 is a front view of a reaction container of a PCR device according to Example 4 of the present invention.

FIG. 6A is an exploded perspective view depicting a configuration of a reaction container of a PCR device according to Example 5 of the present invention.

FIG. 6B is a front view of FIG. 6A.

DESCRIPTION OF EMBODIMENTS

Hereinafter, modes for carrying out the present invention will be described in detail with reference to the accompanying drawings.

EXAMPLE 1

FIG. 1A is an exploded perspective view depicting a configuration of a reaction container of a PCR device according to Example 1 of the present invention, and FIG. 1B is a sectional view of FIG. 1A. FIG. 1B is a sectional view along an AA' plane in the case of combination of FIG. 1A. The PCR

device of the present example includes a channel forming plate **16** and a substrate **21**. The substrate **21** is made of glass, and patterned on an upper surface thereof with an electrode pair **22** prepared by evaporating thin chrome and thereon gold, and the electrode pair **22** has outgoing portions **23** connected by wiring therefrom. The electrode pair **22** has a gap width of 10 μm to 500 μm , for example, 50 μm , and a length of 2 mm to 8 mm, for example, 5.2 mm. The substrate **21** and the channel forming plate **16** form a linear tubular channel **19**. The channel forming plate **16** is made of PDMS (polydimethylsiloxane), disposed by being bonded on the substrate **21**, provided on a lower surface thereof with a groove to form the channel **19**, and provided at one end of the channel **19** with an inlet well **17** of a reaction solution and at the other end with an outlet well **18** of the reaction solution. The channel **19** has, for example, a width of 980 μm , a depth of 600 μm , and the same length as that of the electrode pair **22**. At parts of the substrate **21** being in contact with the inlet well **17** and the outlet well **18** provided at both ends of the channel **19**, through-holes **24**, **25** are opened in the thickness direction, and grommets **28**, **29** are fixed on a lower surface side of the through-holes **24**, **25**. Tubes are connected to these grommets **28**, **29** to let the reaction solution flow in and out.

FIG. 2 is a top view of the reaction container of the PCR device according to Example 1 of the present invention and a view depicting a peripheral configuration thereof. A pump **26** injects the reaction solution through the inlet well **17** into the channel **19**. A pump **27** discharges the reaction solution within the channel **19** through the outlet well **18**. A control section **31** applies an AC voltage necessary for performing a PCR cycle to the electrode pair **22**. The AC has a frequency of 10 kHz to 10 MHz, for example, 5 MHz. As compared with a slight amount of reaction solution within the channel **19**, large electrodes can be used, and a configuration for directly heating the reaction solution is adopted, and thus a time constant of a response of the reaction solution temperature to voltage application can be provided within 1 second.

As PCR cycles, for example, the following steps are repeatedly performed 20 to 30 cycles in order.

- (1) 2 seconds to 10 seconds of denaturation ($\approx 94^\circ\text{C}$.)
- (2) 5 seconds of annealing (54°C . to 60°C .)
- (3) 2 seconds to 10 seconds of extension ($\approx 72^\circ\text{C}$.)

In actuality, a PCR cycle is performed by maintaining an environment surrounding the reaction container at the annealing temperature, and applying in order to reach a denaturation temperature and an extension temperature respectively corresponding AC voltages to the electrode pair **22** to make an AC current flow through the reaction solution and heat the reaction solution by Joule heat to thereby control the temperature of the reaction solution.

Alternatively, a PCR cycle of two steps of performing annealing and extension at the same temperature will suffice.

The present example can carry out any of the following three types of PCR methods. (1) The reaction solution is made to flow continuously or intermittently from the inlet well **17** to the outlet well **18**, while the entire reaction solution within the channel **19** is controlled in temperature so as to be a PCR cycle. (2) With the reaction solution injected in the channel **19** and arrested within the channel **19**, the entire reaction solution is controlled in temperature so as to be a PCR cycle. (3) The electrode pair **22** is divided into several parts, and an AC voltage corresponding to each step of the PCR cycle is always applied to the respective parts of the electrode pair **22**, and the reaction solution is then made to flow continuously or intermittently from the inlet well **17** to the outlet well **18**.

In the present example, because an AC current is made to flow through the reaction solution, the AC current does not

electrolyze the reaction solution. Moreover, because an electric current is made to flow through a gap between the electrodes along a flow of the reaction solution, the electric current flow is wide in width and short in distance and a load resistance is small, and thus even with low application voltage, Joule heat sufficient for temperature control of a PCR cycle can be generated.

Further, when a channel of the present example is used, as online processing, linkage with a previous stage or subsequent stage of processing is possible. As the previous stage, grinding of cells, extraction and purification of genes, fragmentation of cells, or the like is feasible, while as the subsequent stage, an electrophoresis analysis, a microarray analysis, or a connection to a mass spectrometer is feasible, and further various gene analysis methods can be linked as an integrated device that is connected directly at a microchannel without a tube.

EXAMPLE 2

FIG. 3 is a top view of a reaction container of a PCR device according to Example 2 of the present invention and a view depicting a peripheral configuration thereof. For the present example, the reaction container of Example 1 is vertically erected, and the reaction solution is injected from the bottom of the channel **19** and discharged from the top thereof. Because the reaction solution within the channel **19** becomes an upward flow as a result of Joule heating, the reaction solution is sent to flow from the inlet well **17** to the outlet well **18** even without the pumps **26**, **27**. In addition, by using the pumps **26**, **27** in combination, the reaction solution can be sent to flow at a predetermined speed required for a variety of types of PCR methods.

EXAMPLE 3

FIG. 4 is a front view of a reaction container of a PCR device according to Example 3 of the present invention. The PCR device of the present example includes a cover plate **41**, an outlet **42**, an inlet **43**, a channel **44**, an electrode pair **45**, a channel forming plate **46**, and a substrate (not shown in the figure), and the reaction container is vertically erected. Here, the pumps, outgoing portions, and control section are omitted. The channel **44** of the present example has an annular tubular shape. A reaction solution is injected through the inlet **43**. The reaction solution is subjected to Joule heating by the electrode pair **45** to reach a denaturation temperature, and made into an upward flow in the periphery of the electrode pair **45** to circulate within the annular channel **44** so as to perform a PCR cycle. A two-step PCR cycle is assumed here. The reaction solution is discharged through the outlet **42** when the PCR is completed. The present example also uses an upward flow of the reaction solution by Joule heating.

EXAMPLE 4

FIG. 5 is a front view of a reaction container of a PCR device according to Example 4 of the present invention. The PCR device of the present example includes a cover plate **51**, an outlet **52**, an inlet **53**, a chamber **54**, an electrode pair **55**, a chamber forming plate **56**, and a substrate (not shown in the figure), and the reaction container is vertically erected. The cover plate **51** and the substrate are fixed with the chamber forming plate **56** interposed therebetween, and form an upper surface and a lower surface of the chamber **54**, respectively. Here, the pumps, outgoing portions, and control section are omitted. The chamber **54** of the present example forms a flat

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circular space. The electrode pair **55** is provided in the middle of the chamber **54**, and a gap between the electrodes is vertically oriented. A reaction solution is injected through the inlet **53**. The reaction solution is subjected to Joule heating by the electrode pair **55** to reach a denaturation temperature, and made into an upward flow in the periphery of the electrode pair **55** to circulate in two annular forms within the flat chamber **54** so as to perform a PCR cycle. A two-step PCR cycle is assumed here. The reaction solution is discharged through the outlet **52** when the PCR is completed. The present example also uses an upward flow of the reaction solution by Joule heating.

EXAMPLE 5

FIG. 6A is an exploded perspective view depicting a configuration of a reaction container of a PCR device according to Example 5 of the present invention, and FIG. 6B is a front view of FIG. 6A. The PCR device of the present example includes an upper substrate **61**, a lower substrate **62**, a chamber forming plate **63**, a chamber **64**, an electrode pair **65**, an outgoing portion **66**, and an inlet-outlet **67**, and the reaction container is vertically erected. The upper substrate **61** and the lower substrate **62** are fixed with the chamber forming plate **63** interposed therebetween, and form an upper surface and a lower surface (when viewed from the front) of the chamber **64**, respectively. Here, the control section is omitted. One of the electrode pair **65** is disposed on an inner surface of the upper substrate **61**, and the other is disposed on an inner surface of the lower substrate **62**, and the one and the other of the electrode pair compose, with a reaction solution interposed therebetween, an electrode pair that applies voltage across a section in the middle of the chamber. In the front view of FIG. 6B, the electrode pair **65** is disposed so as not to overlap each other. An electric current accordingly flows from edge to edge of the electrode, which reduces variation in resistance of each electric current path flowing over the longitudinal direction of the electrode to reduce variation in electric current, allowing uniform temperature control. The chamber **64** of the present example forms a flat U-shaped space, and includes the inlet-outlet **67** that is vertically opened. A reaction solution is injected through the inlet-outlet **67** by use of a micropipette or the like. Because the chamber is opened at an upper end thereof in the air, the open end is blocked with mineral oil to prevent evaporation of the reaction solution. The reaction solution is subjected to Joule heating by the electrode pair **65** to reach a denaturation temperature, and made into an upward flow in the periphery of the electrode pair **65** to circulate in two annular forms within the flat chamber **64** so as to perform a PCR cycle. A two-step PCR cycle is assumed here. The reaction solution is discharged through the inlet-outlet **67** by use of a glass capillary or the like when the PCR is completed. The present example also uses an upward flow of the reaction solution by Joule heating. In the case of Examples 1 to 4, electric current is made to flow along the substrate, a large amount of heat escapes through the substrate even after heating, but because electric current is made to flow from one substrate to the other substrate in the middle (the thickness direction) of the chamber in the case of the present example, escaping heat can be reduced to perform temperature control with efficiency. Moreover, in the case of the present example, because the distance of a gap between the electrodes is defined by a spacer being the chamber forming plate, no expensive patterning of an electrode pair is necessary, and an electrode pair can be uniformly manufactured at low cost.

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However, the present invention is not limited to the above-described examples.

The material of each component is not limited to the foregoing material, and a component made of a material to be used for a common microchannel can be adopted.

The disclosure of Japanese Patent Application No. 2009-252811, filed on Nov. 4, 2009 including its specification, claims and drawings, is incorporated herein by reference in its entirety.

All the publications, patents and patent applications cited in the present specification are incorporated herein by reference in its entirety.

[Reference Signs List]

41, 51 Cover plate

16, 46 Channel forming plate

17 Inlet well

18 Outlet well

19, 44 Channel

21 Substrate

22, 45, 55, 65 Electrode pair

23, 66 Outgoing portion

24, 25 Through-hole

26, 27 Pump

28, 29 Grommet

31 Control section

42, 52 Outlet

43, 53 Inlet

54, 64 Chamber

56, 63 Chamber forming plate

61 Upper substrate

62 Lower substrate

67 Inlet-outlet

The invention claimed is:

1. A polymerase chain reaction (PCR) method comprising the steps of:

providing, on an inner surface of a container to carry out polymerase chain reaction (PCR), an electrode pair to be disposed to face each other with a gap as part of a flowpath of a reaction solution interposed therebetween; applying an AC voltage to the electrode pair to make an AC current flow through the reaction solution, thereby generating Joule heat to control the reaction solution in temperature;

flowing the reaction solution intermittently through the gap while the entire reaction solution within the container is controlled in temperature so as to be a complete PCR cycle; and

performing a PCR cycle in the container.

2. A polymerase chain reaction (PCR) method comprising the steps of:

providing, on an inner surface of a container to carry out polymerase chain reaction (PCR), an electrode pair to be disposed to face each other with a gap as part of a flowpath of a reaction solution interposed therebetween; applying an AC voltage to the electrode pair to make an AC current flow through the reaction solution, thereby generating Joule heat to control the reaction solution in temperature;

arresting the reaction solution in the container such that the entire reaction solution is controlled in temperature so as to be a PCR cycle; and

performing a PCR cycle in the container.

3. A polymerase chain reaction (PCR) method comprising the steps of:

providing, on an inner surface of a container to carry out polymerase chain reaction (PCR), an electrode pair to be

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disposed to face each other with a gap as part of a flowpath of a reaction solution interposed therebetween; applying an AC voltage to the electrode pair to make an AC current flow through the reaction solution, thereby generating Joule heat to control the reaction solution in temperature; and

performing a PCR cycle in the container,

wherein the electrode pair creates an electric field applied in a perpendicular direction compared to a direction of the flowpath.

4. The PCR method according to claim 1, wherein the container is a tubular channel.

5. The PCR method according to claim 1, wherein the channel is vertically oriented.

6. The PCR method according to claim 1, wherein the container is a flat chamber which is vertically erected, and the electrode pair is disposed to face each other with a vertical gap interposed therebetween on inner surface of one of the sidewalls of the chamber.

7. The PCR method according to claim 1, wherein the container is a flat chamber which is vertically erected, and the electrode pair is disposed to face each other, with the chamber interposed as a gap therebetween, on an inner surface of one of the sidewalls of the chamber and an inner surface of the other sidewall.

8. The PCR method according to claim 2, wherein the container is a tubular channel.

9. The PCR method according to claim 2, wherein the channel is vertically oriented.

10. The PCR method according to claim 2, wherein the container is a flat chamber which is vertically erected, and the

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electrode pair is disposed to face each other with a vertical gap interposed therebetween on inner surface of one of the sidewalls of the chamber.

11. The PCR method according to claim 2, wherein the container is a flat chamber which is vertically erected, and the electrode pair is disposed to face each other, with the chamber interposed as a gap therebetween, on an inner surface of one of the sidewalls of the chamber and an inner surface of the other sidewall.

12. The PCR method according to claim 3, wherein the container is a tubular channel and the channel is vertically oriented.

13. The PCR method according to claim 3, wherein the container is a flat chamber which is vertically erected, and the electrode pair is disposed to face each other with a vertical gap interposed therebetween on inner surface of one of the sidewalls of the chamber.

14. The PCR method according to claim 3, wherein the container is a flat chamber which is vertically erected, and the electrode pair is disposed to face each other, with the chamber interposed as a gap therebetween, on an inner surface of one of the sidewalls of the chamber and an inner surface of the other sidewall.

15. The PCR method according to claim 3, further comprising the step of flowing the reaction solution continuously through the gap while the entire reaction solution within the container is controlled in temperature by the AC current directly heating the reaction solution so as to be a complete PCR cycle.

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